



Jay V. Gonyea¹, Christopher G. Filippi^{2,3}, Angela Applebee², Trevor Andrews^{1,4}, Lindsay Karr⁵, Scott Hipko¹, J.P. Nickerson¹, and Richard Watts¹ ¹Department of Radiology, University of Vermont College of Medicine, Burlington, VT, United States, ²Department of Neurology, University of Vermont College of Medicine, Burlington, VT, United States, ³Department of Radiology, Columbia University Medical Center, New York, NY, United States, ⁴Philips Healthcare, Cleveland, OH, United States, ⁴ ⁵University of Vermont College of Medicine, Burlington, VT, United States

Purpose

To determine if quantitative T_{10} MRI is sensitive to the demyelination process, or protein leakage found in the brains of Multiple Sclerosis (MS) patients^[1], and to compare to normative values of T_{10} in white matter(WM) and cortical gray matter (GM).

Methods

Study Design

- Prospective Cross-Sectional Pilot Study
- 29 MS patients aged 30-60 (43.7 9.2)
- 18 age-matched controls
- MS patient sub-types of: Clinically Isolated Syndrome (10), Relapsing-Remitting (14), Primary Progressive (1), and Secondary Progressive (4) MS



- Data was acquired using a Philips 3T Achieva TX scanner and an 8-channel head coil
- Institutional Review Board (IRB) approval was obtained and all patients were consented Acquisition
- Whole-brain T_{10} -weighted images were acquired using a fluid attenuated variable flip angle 3D turbo spin echo technique (spatial resolution 1.8×1.8×1.8mm³). Images were acquired with a spin lock frequency of 500Hz and spin lock durations of 0, 20, 40, 60, 80 and 100ms.

Analysis

• Each T_{10} map was calculated based on a single exponential fit to the co-registered T_{10} weighted images. The T₁₀ map was then itself co-registered to a T₁-weighted 3D TFE anatomical scan. Using unified segmentation^[2] (SPM8) of the T_1 -weighted image, the T_{10} maps were segmented into WM and GM and spatially normalized to MNI space. Major WM tracts were defined using the JHU atlas^[3], while cortical GM and juxta-cortical WM were defined by an intersection of the Harvard-Oxford cortical atlas (dilated by 5mm) with the subject-specific GM and WM masks respectively. In addition, 3D FLAIR (spatial resolution 1.2x1.2x1.2mm³) and 3D DIR (spatial resolution 1.2x1.2x1.3mm³) images were obtained for lesion identification.

Results

Cortical GM T₁₀ values were higher in all MS groups compared to controls, although this did not achieve statistical significance. WM regions demonstrated significantly higher T₁₀ values in all MS groups compared to controls. Juxta-cortical WM regions were higher in all MS groups, but did not prove significant in the CIS group. The new T_{10} technique produced high SNR whole-brain T₁₀ maps. Figure 1 shows an example of the defined regions-of-interest using the WM/GM segmentation of T_1 weighted image and pre-defined MNI templates. The T_2 -FLAIR shows periventricular lesions that are clearly delineated on the T_{10} map. These lesions demonstrate substantially increased T_{10} (typically 100ms or greater) compared to the surrounding tissue (75-80ms); however, we subtracted the lesions out so that they did not artificially inflate the T_{10} values of the MS groups.

Figure 3. T1-weighted image showing segmentation of cortical gray matter (blue), juxta-cortical white matter (green) and major white matter tracts (forceps minor, cortico-spinal tract, anterior thalamic radiation, inferior longitudinal fasciculus, red);T2-FLAIR showing white matter lesions;T1rho map.

Discussion and Conclusions

T₁₀ MRI has previously been shown to reflect the macromolecular content of biological tissue, due to chemical exchange. Limited brain studies have shown T_{10} to be sensitive to the changes associated with Alzheimer's and Parkinson's disease [4]. MS is known to cause disruption of the blood-brain barrier, which leads to increased levels of blood serum proteins in the brain ^[1]; this

	Controls	CIS-MS	RR-MS	PP-MS	SP-MS	All MS
Sex	6F,11M	7F,3M	10F,4M	1F,0M	2F,*2M	20F,9M
Age (mean)	43.4 10.7	43.2 10.2	41.9 8.9	60	47 4.2	43.7 9.2
Cortical GM (ms)	78.3 1.1	79.0 1.2	79.0 1.2	79.9	78.8 2.2	79.0 1.6
p-value	-	0.185	0.098	n/a	0.661	0.075
WM Tracts (ms)	76.2 1.4	78.9 2.1	78.3 1.8	76.9	79.0 0.9	78.6 1.8
p-value	-	0.003	0.001	n/a	0.002	1.2x10 ⁻⁵
Juxta-Cortical WM	75.1 1.0	76.0 1.3	76.5 1.5	75.5	76.9 0.2	76.4 1.3
p-value	-	0.065	0.005	n/a	1.1x10 ⁻⁶	0.0005
EDSS Score Correlation w/ <u>WM, GM, JC WM</u>		0.14, 0.06,-0.17	-0.14, -0.50,0.18	n/a	-0.10, 0.85,0.52	-0.01, -0.36,0.03

Table 1. Subject demographics and T1rho estimates. (Mean±SD) RR=Relapsing remitting, CIS=Clinically isolated syndrome, PP=Primary progressive. Notes:1 Male SPMS withdrew for claustrophobia.; only 1 PPMS recruited no statistics available for subject.

increase in protein content can increase chemical exchange locally. Abnormal epithelial tight junction (TJ) proteins found in MS could be a possible source of chemical exchange that is detectable with a quantitative MRI measure, like T1p. Our results demonstrate that both normalappearing WM and juxta-Cortical WM have increased T₁₀ values in MS compared to agematched controls. GM did not achieve a statistical difference. Lesions have low signal intensity on the T1-weighted images, leading to their exclusion from the WM/GM masks generated by the segmentation. Thus, our results are not biased by lesion load, which would otherwise increase the T₁₀ values within the defined regions. Including lesions in the analysis would likely increase differentiation between the MS and control groups due to their higher T_{1o} values. In addition, although this study found significant differences between non-focal regions of interest in WM and JCWM, it is possible that specific brain regions show greater changes, which would improve the diagnostic utility of this approach. MS is known to result in early stage cortical lesions, although these lesions are often not visible on standard imaging ^[5,6]. T₁₀ may provide a quantitative measure of juxta-Cortical WM changes that are not seen with other methods. While the differences in T_{10} values is relatively small (~1-2ms), our technique has sufficient sensitivity to detect this subtle change.

Acknowledgements

•Aida Arapovic, Research Coordinator, Department of Radiology, Fletcher Allen Healthcare, Burlington, VT •Steven Braff, M.D., Chairman, Department of Radiology, Fletcher Allen Healthcare, Burlington, VT Jane Low, Research Coordinator, Department of Neurology, Fletcher Allen Healthcare, Burlington, VT •US Department of Energy SC 0001753

References

(1): Haris, M., et al., T1p MRI in Alzheimer's Disease: Detection of Pathological Changes in Medial Temporal Lobe. Journal of Neuroimaging, 2011. p. e86-e90(2):. Ashburner, J. and K.J. Friston, Unified segmentation. Neuroimage, 2005. p.840-851(3): Wakana, S., et al., Reproducibility of quantitative tractography methods applied to cerebral white



multiple sclerosis. New England Journal of Medicine, 2011 p. 2188-2197.

pathology, 2002. 154-169 (5): Filippi, M., et al., Intracorticallesions. Neurology, 2010. p. 19881994. (6). Lucchinetti, C.F., et al., Inflammatory cortical demyelination in early

matter. Neuroimage, 2007. p.839-51(4)Plumb, J., et al., Abnormal endothelial tight junctions in active lesions and normal-appearing white matter in multiple sclerosis. Brain